

Application
for
United States Utility Patent

To all whom it may concern:

Be it known that I,

Leo M. Rozmaryn

have invented certain new and useful improvements in

SYSTEM AND METHOD FOR MEASURING
THE MOTOR STRENGTH OF A HUMAN THUMB OR FINGER

of which the following is a full, clear and exact description:

**SYSTEM AND METHOD FOR MEASURING
THE MOTOR STRENGTH OF A HUMAN THUMB OR FINGER**

RELATED APPLICATION

This application claims priority from U.S. Provisional
5 Application No. 60/428,277, filed on November 22, 2002,
which is incorporated herein by reference.

BACKGROUND OF THE INVENTION

Field of the Invention

The present invention generally relates to a system and
10 method for measuring the motor strength of a human thumb or
finger.

Background of the Invention

Despite great technological advancements in the field of
15 hand surgery over the past twenty-five years, grip and pinch
strength are the only two ways to quantitatively measure
motor strength in the hand. A grip meter can be used to
assess these parameters to make assessments as to focal
areas of strength and weakness in the hand that may be due
20 to primary muscle pathology, nerve and motor end-plate
disease, and/or disorders of bone and joint. Variations in
pinch such as tip, chuck, or key pinch are commonly used to
mimic various activities of daily living. The Medico-Legal
Society and workers compensation communities, as part of
25 disability and return to work assessments, extensively use

hand surgery research, daily clinical practice and the data obtained from grip and strength measurements.

The limitation of grip and pinch tests I have determined lies in the fact that both of these testing modalities evaluate muscle groups that are innervated jointly by the median and ulnar nerves. Grip strength is a composite function with contributions from all the palmar digits, as well as synergistic firing of intrinsic and extrinsic digital flexors. The extrinsic flexors of the sublimis and profundus groups of the hand are dually innervated in the forearm, whereas the intrinsic flexors are primarily ulnarly innervated, and the radial two lumbricals are median innervated.

With pinch strength, the same issues exist. The abductor pollicis brevis is served almost entirely by the median nerve. The adductor pollicis and the first dorsal interosseous are nearly completely ulnarly innervated. The remaining muscles, the flexor pollicis brevis and the opponens pollicis, show wide variations in median and ulnar innervations.

A quantitative measure of forces generated in pure palmar thumb adduction and abduction, I have determined, could serve as an adjunct to grip and pinch strength in the following conditions:

osteo-arthritis pre-operation and post-operation;
rheumatoid arthritis pre-operation and post-operation;

thumb reconstruction after trauma;
reconstruction of congenital differences;
following tendon transfer surgery; and/or
following tumor resection and reconstruction.

5

Instruments that evaluate the function of the human hand
can be divided into three general types. First, instruments
that measure the motor strength of the thumb and fingers in
various positions of pinch and grip. Second, sensory
10 measuring devices that assess fine touch, sharp-dull, two-
point discrimination, pressure and temperature sensation.
Third, dexterity measuring devices that assess neuromuscular
coordination such as pegboard or Moberg instruments.

While existing pinch strength devices assess global
15 functioning of the intrinsic thumb muscles, there is no
known instrument that significantly, substantially and/or
completely isolates one or more muscles that are enervated
by the motor branch of the median nerve. As the motor branch
enters the thenar eminence, I have determined that it
20 enervates the abductor pollicis brevis, the opponens
pollicis, and the superficial head of the flexor pollicis
brevis. Other muscles are powered by the terminal motor
branches of the ulnar nerve. These muscles are the deep head
of the flexor pollicis brevis, the adductor pollicis, the
25 first dorsal interosseous, and some fibers of the opponens
pollicis. The simple act of pinch is actually a complex

interplay of all the above muscles, and therefore there is no way to independently assess the function of those muscles that are enervated by the median nerve alone.

5 Muscles that abduct, or bring the thumb out of the palm in a vector perpendicular to the palm, are innervated by the median nerve. Muscles that adduct, or bring the thumb back toward the palm, are innervated by the ulnar nerve. There is no known device that can measure the force generated by these muscles.

10 For example, one known apparatus for exercising the human hand is described in PCT Publication WO/018018A2, which is incorporated herein by reference. As shown in the schematic illustration of FIG. 1, the assembly 110 includes two major components, a tension member 112 and a compression member 114. The compression member 114 is formed of a
15 resiliently compressible material, such as open cell polyurethane foam, and in the embodiment that is illustrated, is configured as a generally spherical ball 116.

20 The tension member 112 is configured as an elongate, unitary tether 118 formed of a suitable elastomeric material, such as flexible PVC or latex rubber, for example. The tether 118 includes a main cord 120 that extends through a bore 122 in the compressible ball 116. A thumb loop 124 is
25 mounted on the lower end of the main cord so as to project from the bottom of the compressible member, and a

stabilizing web 126 is formed on the upper end of the cord. The stabilizing web protrudes slightly above the upper end of the ball, and finger loops 130, 132, 134 and 136 are attached to the web by comparatively short, narrow elastic
5 cords 140, 142, 144 and 146. The finger cords 140-146 extend from the stabilizing web at predetermined angles so as to develop the correct force vectors for property exercising the hand.

The thumb loop and the finger loops are sized to fit
10 over the middle phalanges of their respective digits, and are also provided with outwardly projecting tab portions 148 which aid in placing the loops by providing a grip for the fingers of the opposite hand.

Tapered junctions 150, 152 are preferably formed where
15 the web and the thumb loop join the main cord. In addition to providing added strength and resistance to tearing in these areas, the tapered junctions 150, 152 engage corresponding recesses 154a, 154b at the ends of the bore 122 through the compressible ball member, thereby providing
20 a firmer, more stable fit between the two members.

Thus, when the exercise assembly is installed on a user's hand, the fingers and thumb are able to move through their full ranges of motion, with the tension member offering a predetermined degree of resistance in the
25 extension-abduction or adduction direction and the compression member providing a predetermined degree of

resistance in the flexion-adduction-opposition direction.
Moreover, the resistance is apportioned properly amongst the
fingers of the hand, and the confirmation of the assembly
ensures that the muscles and tendons are exercised together
5 in a coordinated fashion. In addition, the configuration of
the compressible ball and the tether structure enable the
assembly 110 to be used with either hand, by simply
reversing the assembly and installing the cords on the
corresponding fingers of the other hand.

10 Therefore, the apparatus shown in FIG. 1 in no way
quantitatively measures the forces generated by the thumb in
abduction and adduction.

Summary of the Invention

One embodiment of the present invention provides a system for measuring muscle strength of a human thumb. The system includes a first structure, optionally moveable, that contacts at least a portion of a back side of the hand, and a second structure, optionally in a substantially fixed position, that contacts at least a portion of a palm of the hand. The first and second structures configured to secure the hand in a substantially fixed position. A ring is provided that receives a thumb, and a load cell includes electronics to record a force generated by the thumb. A mechanical assembly is also provided that links the ring and the load cell to transmit the forces from the ring to the load cell.

The mechanical assembly may include a threaded shaft and a nut, with the ring configured to transmit the force generated by the thumb to the threaded shaft and the nut. The mechanical assembly can further include a beam positioned substantially perpendicular to the threaded shaft, with the beam transmitting the load from the threaded shaft to the load cell. The system may also include a knob for rotating the threaded shaft to adjust the position of the nut on the threaded shaft.

In addition, the system may include a push plate, at least one push rod that contacts the push plate and the first structure, a bolt secured to the first structure, and

a handle threaded to negotiate the bolt, wherein upon rotating the handle in a first direction, the push plate, the at least one push rod and the second structure move in a direction to adjustably secure the hand in the substantially
5 foxed position.

 The electronics provides the capability to at least one of: a) display and record forces in at least one of metric and English units; b) display and record a peak force; c) continuously display and record forces generated by the
10 thumb; and d) reset the system prior to a next exertion of force by the thumb. A connection may also be provided that transmits the data recorded by the system to a computing device.

 In another embodiment, the system can include a first
15 plate that contacts at least a portion of a back side of the hand, and a second plate that contacts at least a portion of a palm of the hand. The first and second plates are configured to secure the hand in a substantially fixed position. A ring is provided to receive a thumb of the hand,
20 and a load cell that includes electronics records a force generated by the thumb. A mechanical assembly links the ring and the load cell to transmit the force from the ring to the load cell.

 In another embodiment, a system for measuring muscle
25 strength of a human thumb includes a clamping apparatus to secure a hand in a substantially fixed position, a structure

for receiving a thumb of the hand while the hand is in the substantially fixed position, a force measuring device to record a force generated by the thumb in at least one of abduction and adduction directions, and a mechanical
5 assembly that transmits the force generated by the thumb to the force measuring device. The force measuring device optionally continuously records forces generated by the thumb over a finite period of time. The structure is optionally adjustable with respect to the hand when the hand
10 is in the substantially fixed position.

In another embodiment, a system for measuring muscle strength of a thumb or a finger of a hand is provided that includes a securing apparatus to secure a hand in a substantially fixed position, a structure that is connected
15 to the securing apparatus to receive the thumb or finger of the hand while the hand is in the substantially fixed position, and a force measuring and recording device, responsively connected to the structure, to measure at least one force generated by the thumb or finger in the structure
20 in at least one of abduction and adduction directions, and record the at least one force to be used in at least one of diagnostic and therapeutic treatment of the thumb or finger.

A quantitative measure of forces generated in pure palmar thumb adduction and abduction may serve as an adjunct
25 to grip and pinch strength in the following conditions: a) osteo-arthritis pre-operation and post-operation; b)

rheumatoid arthritis pre-operation and post-operation; c) thumb reconstruction after trauma; d) reconstruction of congenital differences; d) following tendon transfer surgery; and/or e) following tumor resection and

5 reconstruction. In addition, the system significantly, substantially and/or completely isolates one or more muscles that are enervated by the motor branch of the median nerve.

A method for measuring muscle strength of a human thumb in accordance with the present invention includes securing a
10 hand in a substantially fixed position, placing a thumb of the hand in a structure that enables the thumb to generate a measurable force in at least one of the abduction and adduction directions, and recording the force. The method optionally includes providing electronics to record the
15 force generated by the thumb, and providing a mechanical assembly linking the structure to the electronics to transmit the force from the structure to the electronics.

The thumb can move in at least a first direction and a substantially opposing second direction. In addition, the
20 method optionally includes adjusting at least a portion of the structure with respect to the hand.

Further, forces may be displayed in at least one of metric and English units. A peak force generated by the thumb may be displayed, forces generated by the thumb or may
25 be continuously displayed. Recorded forces may be transmitted from the system to a second system.

Another method to measure muscle strength of a thumb or a finger of a hand in accordance with the invention includes at least one of the sequential, non-sequential and sequence independent steps of securing the hand in a substantially fixed position, receiving the thumb or the finger of the hand in a force measuring device, measuring the force generated by the thumb or the finger in at least one of the abduction and adduction directions, and transmitting the force generated by the thumb or the finger to be used in at least one of diagnostic and therapeutic treatment of the thumb or finger. One or more muscles that are enervated by the motor branch of the median nerve are significantly, substantially and/or completely isolated.

Embodiments of the apparatus in accordance with the present invention can thus quantitatively measure, for example, the power of palmar adduction and abduction of the thumb, reflecting the function of median and ulnarly innervated neuro-muscular units separately, thus providing specific information of their integrity.

Embodiments of an apparatus in accordance with the present invention can be used, for example, to measure a degree of motor function in the median nerve in carpal tunnel syndrome and/or the ulnar nerve in ulnar neuropathy, optionally as a preoperative assessment and/or post operative follow up. Patients recovering from injuries to

the median nerve and ulnar nerve, and those who have undergone opponensplasty, can be assessed.

In addition, embodiments of the present invention can be used to test neurological conditions, such as cerebral

5 palsy, stroke victims, and motor wasting conditions such as Charcot-Marie-Tooth, which affect the intrinsic muscles of the hand. The ability to abduct and adduct the thumb is affected by basal joint arthritis, and the difference

10 between pre- and post-operative abductor and adductor strength can be one indicator of success. Embodiments of the invention can also include an isokinetic mode that allows controlled motion with varying loads that can assist in muscle conditioning of the thumb.

15 In view of the foregoing, it should be apparent that embodiments of the present invention can advantageously be used, for example, in the following clinical specialties:

Orthopaedic and Plastic Hand Surgeons;

Orthopaedic Surgeons;

Physical Medicine and Rehabilitation Medicine

20 Physicians;

Physical and Occupational Therapists;

Neurologists;

Rheumatologists;

Family Practice Physicians;

25 Osteopaths; and/or

Chiropractors.

There has thus been outlined, rather broadly, the features of the invention in order that the detailed description thereof that follows may be better understood, and in order that the present contribution to the art may be better appreciated. There are, of course, additional features of the invention that will be described hereinafter and which will form the subject matter of the claims appended hereto.

In this respect, before explaining at least one embodiment of the invention in detail, it is to be understood that the invention is not limited in its application to the details of construction and to the arrangements of the components set forth in the following description or illustrated in the drawings. The invention is capable of other embodiments and of being practiced and carried out in various ways. Also, it is to be understood that the phraseology and terminology employed herein are for the purpose of description and should not be regarded as limiting.

As such, those skilled in the art will appreciate that the conception, upon which this disclosure is based, may readily be utilized as a basis for the designing of other structures, methods and systems for carrying out the several purposes of the present invention. It is important, therefore, that the claims be regarded as including such

equivalent constructions insofar as they do not depart from the spirit and scope of the present invention.

These together with other objects of the invention, along with the various features of novelty which
5 characterize the invention, are pointed out with particularity in the claims annexed to and forming a part of this disclosure. For a better understanding of the invention, its operating advantages and the specific objects attained by its uses, reference should be had to the
10 accompanying drawings and descriptive matter in which there is illustrated preferred embodiments of the invention. Other features of the present invention will be evident to those of ordinary skill, particularly upon consideration of the following detailed description of the preferred
15 embodiments.

Brief Description of the Drawings

The detailed description of the present application showing various distinctive features may be best understood when the detailed description is read in reference to the appended drawing in which:

FIGS. 1 is a diagram illustrating a conventional apparatus for exercising the human hand;

FIG. 2A is a first perspective view of an exemplary apparatus in accordance with the present invention;

FIG. 2B is a second perspective view of the apparatus shown in FIG. 1A;

FIG. 3 is a side view of the apparatus shown in FIGS. 2A and 2B;

FIG. 4 is an exemplary embodiment of a shaft that can be utilized in connection with the present invention;

FIG. 5 is an end view of FIG. 3.

FIG. 6 is a top sectional view of FIG. 3, showing a load cell mount.

FIG. 7A is a top sectional view of the ring plate.

FIG. 7B is an elevation view of the ring plate.

FIGS. 8A and 8B show a second exemplary embodiment of the present invention.

FIG. 9 is a flow diagram of an exemplary method in accordance with the present invention.

FIG. 10 is an exemplary circuit diagram of an edge connector that can be used in connection with the present invention.

FIG. 11 is a diagram of exemplary force circuitry that can be used in connection with the present invention.

FIG. 12 is a diagram of exemplary auto tare circuitry that can be used in connection with the present invention.

FIG. 13 is a diagram of exemplary peak hold circuitry that can be used in connection with the present invention.

FIG. 14 shows various exemplary electronics that can be used with power activation and deactivation in connection with the present invention.

FIG. 15 shows various exemplary electronics that can be used with force measurement in connection with the present invention.

FIG. 16 is a data table showing age, weight and sex characteristics for right dominant subjects.

FIG. 17 is a data table showing abduction strength for right dominant males and females by joint age and weight.

FIG. 18 is a data table showing abduction strength for left dominant males and females by joint age and weight.

FIG. 19 is a data table showing adduction strength for right dominant males and females by joint age and weight.

FIG. 20 is a data table showing adduction strength for left dominant males and females by joint age and weight.

FIG. 21 is a data table showing grip strength by age and weight for both left and right dominant males and females.

FIG. 22 is a data chart showing right dominant male abduction strength by age at 30, 45 and 60 degree positions.

5 FIG. 23 is a data chart showing right dominant female abduction strength by age at 30, 45 and 60 degree positions.

FIG. 24 is a data chart showing right dominant male abduction strength by weight at 30, 45 and 60 degree positions.

10 FIG. 25 is a data chart showing right dominant female abduction strength by weight and age at 30, 45 and 60 degree positions.

FIG. 26 is a data chart showing right dominant male abduction strength by age at 30, 45 and 60 degree positions.

15 FIG. 27 is a data chart showing right dominant female abduction strength by age at 30, 45 and 60 degree positions.

FIG. 28 is a data chart showing right dominant male abduction strength by weight at 30, 45 and 60 degree positions.

20 FIG. 29 is a data chart showing right dominant female abduction strength by weight at 30, 45 and 60 degree positions.

FIG. 30 is a data chart showing the ratio of male grip strength to abduction strength by age at 30, 45 and 60 degree positions.

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FIG. 31 is a data table showing correlation coefficients for all subjects by sex, age and weight at 30, 45 and 60 degree positions.

Detailed Description of the Invention

Reference now will be made in detail to the presently preferred embodiments of the invention. Such embodiments are provided by way of explanation of the invention, which is not intended to be limited thereto. In fact, those of ordinary skill in the art may appreciate upon reading the present specification and viewing the present drawings that various modifications and variations can be made.

For example, features illustrated or described as part of one embodiment can be used on other embodiments to yield a still further embodiment. Additionally, certain features may be interchanged with similar devices or features not mentioned yet which perform the same or similar functions. It is therefore intended that such modifications and variations are included within the totality of the present invention.

As illustrated, for example, in Figures 2-8, embodiments of the present invention are directed to an apparatus 200 for measuring forces generated by a human thumb. A base 202 is shown, having a bottom plate 204, a top plate 206, and sides. Top plate 206 and bottom plate 204 are secured to base 202 by any suitable known securing means, such as bolts 232, which are located at each corner of base 202. Base 202 includes a display 210 for displaying measured thumb forces, and switches 208a-f, as shown in FIGs. 2A and 2B. Switch 208a can be used to display the force exerted by the thumb

on display 202, on a display (not shown) on an opposing side of base 202, or both displays. Switch 208b can be used to select force measurement in either pounds or kilograms.

Switch 208c can be used to select to display a peak or

5 maximum force, or a continuously updated display of measured force. Switch 208d can be used to zero out the forces

between recordings. Switch 208e is used to turn the

apparatus on and off. Finally, switch 208f can be used to

select either abduction (i.e., movement away from the palm

10 of the hand) or adduction (i.e., movement toward the palm of the hand) movement of the thumb.

Vertical housing 214 can be used to house beam 318 and related structure, as will be discussed with regard to FIG.

3. Ring plate 220 carries ring 222, as will be discussed in

15 further detail herein. Various inserts or sizers can be attached to ring 222 to accommodate various thumb sizes. For example, inserts or sizers can snap on to ring 222, or be secured thereto using, for example, velcro. Ring plate 220 and vertical housing 214 can be secured to top plate 206

20 using any suitable known securing means, such as bolts 234a, 234b. Alternative means to secure ring plate 220 may optionally be used.

Stationary plate 218 can be interposed between ring plate 220 and top plate 206, and can be secured to ring

25 plate 220 and top plate using any suitable securing means, such as bolts 236. Bolts (not shown) that protrude through

top plate 206 can be used to secure a bottom portion of stationary plate 218 to top plate 206. A user's hand is positioned between hand plate 216 and stationary plate 218, with the palm of the user's hand contacting stationary plate 218, and the back of the user's hand contacting hand plate 216. Hand plate 216 can optionally have a soft material affixed thereto, such as foam, cloth, and the like, to increase user comfort. Alternative structures to position the user's hand may optionally be used.

Push plate 212 mates or is connected to a first end of a plurality of tubes 224. A second end of the plurality of tubes 224 mates or is connected to a proximal face (e.g., closest to handle 228) of hand plate 216. Handle 228 is threaded to engage bolt 226 such that when handle 228 is turned in a first direction (e.g. clockwise), push plate 212, tubes 224 and hand plate 216 move toward stationary plate 218 to secure a user's hand, which is positioned between hand plate 216 and stationary plate 218, in a substantially fixed position. When handle 228 is turned in a second direction (e.g., counterclockwise), push plate, tubes 224 and hand plate 216 can be moved away from the user's hand, and thereby permit removal of the hand. Tubes 224 are preferably arranged with respect to push plate 212 and hand plate 216 in a manner such that each tube bears substantially the same load when hand plate 216 engages a

user's hand. Pivot 240 will be described with regard to FIG. 3.

FIG. 3 is a side view of the apparatus shown in FIGs. 2A and 2B. Shaft 302 can be a threaded shaft that engages bolt 308. Ring 222 can be secured to bolt 308 in a conventional manner. For example, corresponding holes can be provided in bolt 308 and ring 222 such that ring 222 can be secured to bolt by a rivet or threaded connection. Bearing shafts 304a, 304b are also engaged with shaft 302. A more detailed figure of shaft 302 and bearing shafts 304a, 304b is shown in FIG. 4. Shafts 302, 304a, 304b can be stainless steel. Shaft 302 can have holes drilled for bearing shafts 304a, 304b, and bearing shafts 304a, 304b can be secured to shaft 302 using, for example, a Loctite® adhesive.

Ball bushings 306a, 306b respectively receive shafts 304a, 304b. Knob 230 is connected to bearing shaft 304b such that when knob 230 is turned in a first direction (e.g. clockwise), bolt 308 moves in a first direction (e.g., toward knob 230). When knob 320 is turned in a second direction (e.g., counterclockwise), bolt 308 moves in a second direction (e.g., away from knob 230). Knob 230 thus facilitates adjusting the position of ring 222.

A first end of beam 318 is operatively engaged with or affixed to bearing shaft 304b. A second end of beam 318 is operatively engaged with or affixed to shaft 316 which, in turn, is operatively engaged with or affixed to load cell

312. Load cell 312 can house electronics such as shown in
Figs. 11-14. Mount 314 can be secured to bottom plate 204,
and a portion of load cell 312. Caps 320a, 320b can be
respectively secured to an end of bearing shaft 306b and
5 shaft 316 to facilitate holding beam 318 substantially in
place. Padding 310 is shown contacting hand plate 216. Top
plate portions 206a, 206b are shown, which provide a space
for beam 318. Shaft 240 is provided to enable the force by
the user's thumb received at an upper portion 318a of beam
10 318 to transfer to a lower portion 318b of beam 318, and
subsequently to load cell 312.

In operation, the apparatus 200 is configured so that a
hand (not shown) is held in a neutral position in the
pronation-supination plane. The user can sit with his or her
15 hand inserted between hand plate 216 and stationary plate
218. The hand can be inserted until the mid-palmar crease of
the hand reaches plate 218. The thumb is inserted into thumb
ring 222, which can be adjusted to be positioned at a
desired distance from plate 218.

20 Handle 228 can be rotated to secure plate 216 against
the hand. Thumb ring 222 can be attached to nut 308 which,
in turn, is secured to shaft 302. Thumb ring 222 can be
adjusted toward or away from stationary plate 218 by turning
adjustable knob 230. For example, turning knob 230 can
25 rotate shaft 302 such that nut 308 can negotiate shaft 302
as it is turning. Accordingly, the position of nut 308 and

thumb ring 222 can be adjusted within the stationary plate 218.

Shaft 302 is operatively configured to operate with a strain gauge, or similar force measuring device, within load cell 312 to record forces generated by the thumb. In an embodiment, there is no observable movement in ring 222 (and thus shaft 302 and/or beam 308) when thumb force is exerted by a user. Load cell 302 can be supplied with a constant low voltage, which is nulled by adjustment circuitry such as shown in FIG. 15 when no thumb force is present. When thumb force is applied, there is an output voltage change, positive or negative, which is amplified and converted to a digital readout showing force, as pounds or kilograms, in display 202.

Depending on the position of adjustable ring 222, different forces can be generated by the thumb. Accordingly, there is a distance of ring 222 from the hand that enables the thumb to generate maximum forces. Forces generated by the thumb are transferred to shaft 302, 306a, 306b, and to load cell 312.

In addition, display 210 or the display (not shown) on the opposing side of base 202 can optionally be blacked out by using switch 208a, so that the user does not see the display of thumb force generated during. Display 210 can be a digital display, optionally connected with, for example, a Windows®-based software program that can plot a "force

versus time" curve to detect muscle fatigue. For example, cable 242 can be used to transmit recorded forces to a Windows®-based software program that can plot, for example, a force versus time curve.

5 Deviations from normal measurement can be used to assess differing disease states, such as in carpal tunnel syndrome and/or isolated injuries to, for example, the median and/or ulnar nerve.

10 It is preferred that the wrist is held at 35° of extension, and that the palmar digits are kept in full extension at the metacarpal-phalangeal (MP), proximal interphalangeal (PIP), and distal interphalangeal (DIP) joints. The thumb can be positioned at the level of the inter-phalangeal joint, and then inserted into the ring 222.

15 The static angle of thumb abduction can be assessed with a goniometer at, for example, 30, 45 and 60 degrees. Other degrees of extension are also possible, for example, ranging between 15 degrees and 55 degrees, or full extension and/or flexion.

20 FIG. 5 is an end view of FIG. 3, showing beam 318. Tube holes 502a-d are shown, which respectively receive or contact a tube 224, as shown in FIGs, 2A and 2B.

25 FIG. 6 is a top sectional view of FIG. 3, showing an exemplary positioning of load cell mount 314 within base 202.

FIG. 7A is a top sectional view of ring plate 220,
viewed in the direction of cut A-A as shown in FIG. 3. FIG.
7B is an elevation view of ring plate 220. Spaces 704a, 704b
are respective spaces for ball bushings 306a, 306b. Space
5 702 receives shaft 302 and bolt 308. Space 706 receives the
top portion of beam 318 and cap 320a.

FIGs. 8A and 8B, generally at 800, show a second
exemplary embodiment of the present invention. Platform 802
is provided, which contacts a lower portion 808a of
10 stationary hand rest 808. An interface portion 808b of hand
rest 808 can receive an extended portion 810a of moveable
hand rest 810. Extended portion 810a can also be a piece
that is separate from hand rest 810. Extended portion 810a
can optionally move into and away from interface 808b to
15 secure a user's hand, as shown in FIG. 8B.

Spring guide 808c is positioned between interface 808b
and mount 808d. Standard electronics similar to that shown
in FIGs. 10-15, and related structure can be housed in mount
808d. The force exerted by the user's thumb on ring 804a can
20 be displayed on display 806. Ring 804a can be connected to
spring 812 in various positions, as shown at 804b, 804c. In
the embodiment shown in FIGs. 8A and 8B, spring 812 can be
used in lieu of bearing shafts 304a, b and respective ball
bushings 306a, 306b, and bolt 308 shown, for example, in
25 FIG. 3. Spring 812 preferably has a sufficiently high spring
constant such that no visible movement of spring 812, and

thus ring 804a, is apparent when a user exerts force on ring 804a.

The forces created in the spring is transferred to a load cell and calibrated strain gauge (not shown), which can be housed in display mount 808d in a manner similar to that shown in FIG. 3. Switches (not shown) can be provided in a manner similar to that shown, for example, in FIGs. 2A and 2B to select the direction in which thumb force is being applied, select force measurement in either pounds or kilograms, select a peak force, and/or select a continuously updated display of measured force. In addition, display 806 can be selectively blacked out so that apparatus 800 can be used in a blinded fashion with respect to the patient. Display 806 can be connected to and/or configured to operate with, for example, a Windows®-based software program, optionally running on a separate computing device, that can plot, for example, a thumb force versus time curve.

FIG. 9 is a flow diagram of an exemplary method in accordance with embodiments of the present invention. The method described with regard to FIG. 9 is also applicable to the embodiment shown in FIGs. 8A and 8B, but will be described with regard to FIGs. 2A and 2B. Note that the method described in FIG. 9 is exemplary, and may performed in different orders and/or sequences as dictated by the apparatus of the present invention, and any alternative embodiments of the apparatus. In addition, the method

described herein is not limited to the specific use of the apparatus of the present invention, but may be performed using any apparatus that is capable of obtaining the information as described in connection with the apparatus of the present invention.

At step 902, a user positions his hand and four fingers in the apparatus 300, between hand plate 216 and stationary plate 218 shown in FIGs. 2A and 2B. Other sequences of the method are also within the scope of the present invention.

At step 904, the user's thumb is positioned in ring 222 and, at step 906, the abduction or adduction mode is selected. At step 908, the user exerts thumb force and, at step 910, the forces by the thumb are recorded. At decision step 912, a determination is made whether to display the force(s) on display 210. If the forces are to be displayed, at step 914 the forces can be displayed on display 220. If at decision step 912 it is determined that forces are not to be displayed, and after step 914, a determination is made whether to perform an additional force measurement. If another force measurement is performed, the process returns to step 906. If no additional force measurements are to be taken, the process ends.

FIG. 10, generally at 1000, is an exemplary and standard circuit diagram of an edge card 1000 connector that can be used in connection with a personal computer (not shown) that receives data from the apparatus 200, 800. Cable 242

connected to apparatus 200, 800 can interface with the edge card 1000 to transfer data to the computer.

FIG. 11, generally at 1100, is a diagram of exemplary and standard force circuitry that can be used in connection with the present invention to record forces generated by a user's thumb. The circuitry can be located in load cell 312.

FIG. 12 is a diagram of exemplary and standard circuitry that can be used to record peak forces generated by a user's thumb. The circuitry can be located in load cell 312.

FIG. 13 is a diagram of exemplary and standard peak hold circuitry that can be used in connection with the present invention. The circuitry can be located in load cell 312.

FIG. 14 shows various exemplary and standard electronics that can be used with power activation and deactivation in connection with the present invention, in connection with switch 208e. The circuitry can be located in load cell 312.

FIG. 15 shows various exemplary and standard electronics that can be used with force measurement in connection with the present invention. The circuitry can be located in load cell 312.

Emperical Testing and Results

Six hundred patients between the ages of ten and seventy years of age were tested using the apparatus 200. Patients were divided into seven age groups according to decade, with equal numbers of males and females. Patients in each age

group were stratified according to eight weight classes ranging from fifty to three hundred pounds. Hand dominance as well as the value of mid range grip (third position on the Jamar dynamometer) was recorded. Each subject was asked
5 as to whether they ever had any injuries or surgery to their hand and as to the presence of any symptoms in their hands such as numbness, tingling, weakness or pain in their hands. A positive answer to any of the above questions disqualified the subject from taking the test.

10 Both hands were then sequentially placed into the apparatus 200, and secured into place. The values for abduction and adduction strength were recorded at the 30, 45, and 60-degree positions, and comparisons between these values are made. Correlations of results as to age, weight,
15 and hand dominance and grip strength were assessed and recorded.

There were two hundred ninety four males of which 93% were right hand dominant. Of the three hundred six females, 91% were right handed. In both groups the numbers of
20 patients were evenly distributed for each age range from 10-70 years old. The vast majority of patients fell within the 125-200 pound weight range (FIG. 16). However it is noted that within each age class there were wide variations in weight. For each parameter of age and weight, a specific
25 mean value for abduction and adduction and grip strength can be assigned (FIGs. 17-20). Using a standard reference

manual, one can determine for any age and weight parameter what the mean and standard deviation for grip, adduction, and abduction are and a given patient can be compared against this data.

5 Grip strength in men increases to a peak between 25-40 years old to 120 pounds, and slowly decreases to 90 pounds by age 75. Within each age class, the grip can vary by as much as 35 pounds, but in general follows the curve of averages (FIG. 21). This holds true for right and left
10 hands.

 The curve for females is much flatter than males, with averages from 60-80 pounds. Within each age class there is variability by weight class by as much as 30 pounds. There is no significant difference between right and left hands.

15 Looking specifically at abduction as a function of age for males, right hands are consistently but not significantly stronger than left hands. There is a tri-modal curve with peaks at age 25, 37, and 53 years old. At 30° abduction, this approaches 5.8 pounds. The strength of
20 abduction decreases as the starting position of abduction increases from 30 to 45 and to 60 degrees (FIG. 22).

 For females, abduction strength rises to three pounds by age 24, and remains constant throughout life (FIG. 23). The strength of abduction decreases as the starting position of
25 abduction increases. Within each age group there is

significant variability according to weight, which is more apparent in males than females.

If the data is broken down according to weight, for males, there is a steady rise in abduction, with weight leveling off at 225 pounds with 6.0 pounds of force. As the starting position of abduction increases from 30 to 45 to 60°, the power of abduction diminishes. Also the right dominant hand is stronger than the left hand (FIG. 24). For females, there is a rise in abduction with weight to 3.2 pounds of force, but less dramatic than with males (FIG. 25).

For male adduction, there is a tri-modal distribution with peaks at 27, 37, and 53 years of age. At 60° thumb abduction angle, maximal adduction strength is 21.5 pounds of force, which occurs at age 27. With increasing abduction angle the strength of adduction increases. The right hand is stronger than the left hand, but not significantly so (FIG. 26).

For females, the curves are flatter than males after age 24 (FIG. 27). There is increased strength of adduction with increased thumb abduction angle. Peak strength occurs at 55-59 years of age at 16.5 pounds.

If adduction data is examined by weight, a similar pattern emerges. For males there is a steady increase by weight class, leveling off at 225 lbs with 20.5 pounds of force. There is little variation between right and left

hand. As the abduction setting increases from 30 to 45 to 60 degrees, the adduction strength increases (FIG. 28). Females have the same curve as males, but the curve is much flatter and levels off at 180 lbs with 16.2 pounds of force (FIG. 29).

It is instructive to correlate adduction and abduction to grip strength. The ratio of grip to adduction is linear, and age and abduction angle independent. The relationship to abduction fluctuates with age, varies between the right hand and left hand, and abduction angle. The pattern applies to both males and females (FIG. 30).

This data supports the study of correlation coefficients. There is a low correlation between adduction/abduction and grip, and between adduction/abduction and age and weight. There is a moderate correlation between adduction/abduction and right and left grip. Finally, there is a moderate to high correlation between right and left hand adduction/abduction (FIG. 31).

The many features and advantages of embodiments of the present invention are apparent from the detailed specification, and thus, it is intended by the appended claims to cover all such features and advantages of the invention which fall within the true spirit and scope of the invention. Further, since numerous modifications and variations will readily occur to those skilled in the art,

it is not desired to limit the invention to the exact construction and operation illustrated and described, and accordingly, all suitable modifications and equivalents may be resorted to, falling within the scope of the invention.